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# Combining ultrasound directed self-assembly and stereolithography to fabricate engineered polymer matrix composite materials with anisotropic electrical conductivity

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ARTICLE INFO	A B S T R A C T		
Keywords: Ultrasound directed self-assembly Conductive composites Polymer matrix Composites Additive manufacturing	Engineered polymer matrix composite materials with designer electrical properties are important for a myriad of engineering applications including flexible electronics, electromagnetic shielding, and materials with embedded electrical wiring. However, existing fabrication methods are limited by material choice and dimensional scal- ability. We use the acoustic radiation force associated with a standing ultrasound wave field to spatially arrange and align electrically conductive microfibers dispersed in a photopolymer matrix in user-specified orientations and use stereolithography to solidify the material. We relate the electrical conductivity of the material specimens to the fabrication process parameters, including ultrasound transducer power, microfiber alignment, and mi- crofiber weight fraction. Logistic regression analysis demonstrates that the probability that a composite material specimen is electrically conductive increases with increasing microfiber weight fraction and microfiber align- ment because these parameters drive the formation of a long-range percolated network of electrically conductive microfibers. We determine that the electrical conductivity of conductive specimens ranges between 31 – 793 S/m and that the fabrication process parameters are critical in predicting whether a composite material specimen is electrically conductive or insulating. Relating the composite material fabrication process parameters to the resulting electrical properties for use in engineering applications. The combined ultrasound DSA and SLA fabrication process works independent of fiber and matrix material properties and facilitates dimensional scal- ability due to low attenuation of ultrasound waves in viscous media.		

## 1. Introduction

Polymer matrix composite materials consist of a polymer matrix and one or more continuous or discontinuous filler materials [1]. Continuous filler material (e.g., fiber tow) typically spans the entire length of the composite material specimen, aligns under mechanical tension during the fabrication process, and serves as mechanical reinforcement to the polymer matrix [2]. Discontinuous filler material may consist of microor nanosized particles such as microfibers [3], microrods [4], nanofibers [5], carbon nanotubes (CNTs) [6], or powders consisting of spherical particles [7], to name a few. They either randomly disperse [8] or align in a specified pattern in the polymer matrix [9]. Changing the material properties, weight fraction, and alignment of the discontinuous filler material in the polymer matrix affects the bulk properties of the polymer matrix composite material and how it interacts with an external field (e. g., electric, magnetic, force fields). Thus, these materials can be engineered to display a variety of properties, including designer thermal [10], mechanical [11], or electrical [12] properties. In this paper, we specifically focus on electrical conductivity or, correspondingly, electrical resistance. For instance, aligning electrically conductive filler material in the composite material matrix can function as embedded electrical wiring [13], which is useful to a myriad of engineering applications, including flexible electronics [14], chemical or biological sensors [15], and stretchable strain sensors [16].

We determine the electrical conductivity of a polymer matrix composite material from an electrical resistance measurement, which depends on the electrical properties of the matrix and filler materials [17], and the concentration [18], size [19], and alignment [12] of the filler material within the matrix material. Several methods exist to quantify the electrical resistance of polymer matrix composite materials with

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discontinuous filler material. A DC electrometer allows precision high-resistance measurements, but typically only above  $10^3$  Ohm, thus rendering it unsuitable for electrical conductors [20]. An impedance analyzer measures impedance as a function of frequency, and is typically used to measure AC electrical conductivity [21]. A parameter analyzer measures the DC current as a function of voltage magnitude (max. 10V), which makes it suitable for conductors and semiconductors [12]. Finally, using a high-quality multimeter to measure DC resistance is straightforward and accurate for conductors and semiconductors [22].

Fabricating polymer matrix composite materials with designer electrical properties or embedded electrical wiring requires creating percolated networks of aligned filler material that enable electrical current between different locations in the material. The percolation threshold is defined as the minimum weight fraction of discontinuous filler material that forms long-range connectivity in the material specimen [23]. (Partially) aligning uniformly distributed discontinuous filler material reduces the percolation threshold compared to random or isotropic alignment [24]. Spatially arranging and aligning discontinuous filler material increases the local filler material density and, thus, the probability that individual filler material particles make contact, which decreases the percolation threshold [5], increases electrical conductivity in the alignment direction [25], and decreases electrical conductivity transverse to the alignment direction [26], compared to composite material specimens with randomly oriented (electrically conductive) discontinuous filler material.

Fabricating polymer matrix composite materials with aligned discontinuous filler material requires combining a technique to form the macroscale material specimen geometry with a method to spatially arrange and align filler material within the polymer matrix [27]. Conventional fabrication methods, such as mold casting [28], typically inject a mixture of liquid polymer matrix and filler material into a hollow cavity. Alternatively, additive manufacturing (AM) methods such as stereolithography (SLA), fused filament fabrication (FFF) or fused deposition modeling (FDM), and direct ink writing (DIW) enable the formation of complex free-form geometries in a layer-by-layer fashion without the need for a mold [29]. Our group recently published a comprehensive review on this topic [27].

Several methods exist to spatially arrange and align discontinuous filler material within a polymer matrix material. Researchers have demonstrated that filler material can orient in the direction of an electric [30] or magnetic [31] field, or a combination of both [32]. However, this requires an electrically conductive or ferromagnetic filler material (or coating) and a large external field strength (on the order of 20 kV/m [33] and 8000 mT [34], respectively), which limits dimensional scalability. Khan et al. used a DC electric field within a mold to align multi-walled CNTs (MWCNTs) in epoxy and showed increased electrical conductivity in the alignment direction compared to specimens with randomly oriented MWCNTs [35]. They also documented that electrical conductivity increased with increasing filler material weight fraction. Oliva-Avilés et al. showed anisotropic electrical conductivity in polymer matrix composite materials with CNT filler material that was aligned using an AC and DC electric field, and also documented that electrical conductivity increased with increasing CNT weight fraction [25]. Ma et al. used a magnetic field to align CNTs in epoxy and measured that the electrical conductivity was higher in the direction parallel, as opposed to perpendicular, to the aligned CNTs and also increased with increasing CNT weight fraction [36].

Shear force fields, created by viscous flow of the matrix material with dispersed filler material, typically align filler material in the direction of shear but cannot manipulate spatial arrangement, which limits control over the local filler material density and, thus, the electrical properties of the resulting composite material. Postiglione et al. used DIW in combination with a shear force field, and a mixture of polylactic acid (PLA) and electrically conductive MWCNTs, to 3D print electrically conductive polymer matrix composite materials with aligned MWCNTs [37]. They reported that electrical conductivity increased with

increasing MWCNT weight fraction and identified the minimum MWCNT weight fraction required for long-range electrical conductivity.

Ultrasound directed self-assembly (DSA) relies on the acoustic radiation force associated with a standing ultrasound wave field to spatially arrange [38] and orient [39] filler material, independent of material properties or shape [40]. Furthermore, standing ultrasound wave fields display low attenuation in low-viscosity fluids [41], which enhances dimensional scalability compared to other external fields. Melchert et al. fabricated flexible polymer matrix composite materials with ultrasonically aligned carbon and silver-coated glass microfibers, and demonstrated anisotropic electrical conductivity compared to specimens with randomly oriented microfibers [42]. Yunus et al. used a standing ultrasound wave field to align several types of filler material, including copper and magnetite nanoparticles and carbon nanofibers in photocurable polymer [7]. They measured that the electrical conductivity of the resulting composite material increased with increasing filler material weight fraction and depended on the electrical conductivity of the filler material. Greenhall and Raeymaekers used SLA and a standing ultrasound wave field to 3D print photocurable polymer matrix composite materials with aligned nickel-coated carbon microfibers and measured electrical resistance on the order of  $10^6$  times larger in the direction perpendicular compared to parallel to the microfiber alignment [13].

Table 1 summarizes the literature on fabricating electrically conductive polymer matrix composites materials with discontinuous filler material aligned by means of an external electric, magnetic, shear force, or ultrasound wave field.

The literature documents several methods of fabricating polymer matrix composite materials with percolated networks of electrically conductive microfibers. However, to fabricate polymer matrix composite materials with designer electrical conductivity, one must relate the alignment and orientation of the filler material and its corresponding electrical conductivity or resistance, to the fabrication process parameters. This paper specifically focuses on the combination of SLA and ultrasound DSA because ultrasound functions independent of the filler and matrix material properties and SLA allows selectively curing photopolymer to fixate the filler material in place, without the need for a mold. Thus, this technique offers materials flexibility and dimensional scalability.

The objective of this paper is to characterize the electrical conductivity of polymer matrix composite material specimens as a function of the ultrasound DSA fabrication process parameters, including ultrasound transducer power, microfiber alignment, and microfiber weight fraction. We use multivariate logistic regression analysis to derive a bestfit model that relates whether a polymer matrix composite material specimen conducts electricity to its fabrication process parameters. Additionally, we attempt to relate the electrical conductivity of electrically conductive material specimens to the fabrication process parameters. We present the results in non-dimensional fashion to render them independent of our specific experiment. These results have importance to devising a fabrication process based on standing ultrasound waves and additive manufacturing, which enables implementing polymer matrix composite materials with designer electrical properties for specific engineering applications.

#### 2. Methods

#### 2.1. Fabricating electrically conductive composite material specimens

Fig. 1 schematically shows the experimental apparatus, previously developed by our research group to integrate ultrasound DSA and SLA [13], which we use to fabricate engineered composite material specimens that contain parallel lines of aligned, electrically conductive silver-coated glass microfibers (weight fraction  $1.0 \le w_f \le 4.0\%$  - measured when mixing the microfibers with the matrix, average diameter 15 µm, average length 130 µm, density 1000 kg/m<sup>3</sup>, Potters

#### Table 1

Overview of external field-based alignment methods of discontinuous filler material in electrically conductive polymer composite materials, identifying specific references, and showing compatible polymer matrices, filler materials, filler material weight fraction  $w_{f_i}$  filler material alignment quantification methods, and reported electrical conductivity range. We use the following abbreviations: Polyvinylidene fluoride (PVDF), polysulfone (DPSF), polylactic acid (PLA), carbon nanofibers (CNFs), graphene nanoplatelets (GNPs).

	Electric field	Magnetic field	Shear force field	Ultrasound wave field
Polymer matrix material	<ul> <li>Epoxy [5,22,35,43, 44]</li> <li>PVDF [12]</li> <li>DPSF [25]</li> </ul>	• Epoxy [26,36,44]	• PLA [37]	• Photopolymer [7,13,42,45]
Filler material	<ul> <li>CNTs [12,25,44]</li> <li>CNFs [5,22,43]</li> <li>GNPs [5]</li> <li>MWCNTs [35]</li> </ul>	• CNTs [36,44] • GNPs [26]	• MWCNTs [37]	<ul> <li>Ni-coated microfibers [13,45]</li> <li>Ag-coated microfibers [42]</li> <li>Carbon microfibers [42]</li> <li>Magnetite and copper nanoparticles [7]</li> <li>CNFs [7]</li> </ul>
Filler material w <sub>f</sub> [%]	0.05 [35] - 3.0 [44]	0.5–5.0 [36]	0.5-10.0 [37]	0.5–9.0 [7]
Filler material alignment quantification method	N/A	ImageJ open source software [36]	N/A	FFT anisotropy [13]
Electrical conductivity $\kappa$ [S/m]	$4 \cdot 10^{-3}$ [44] – 0.8 [12]	$10^{-9}$ [26] – 4.10 <sup>-3</sup> [36]	50 [37]	4.38·10 <sup>-13</sup> [7] - 5000 [42]



**Fig. 1.** (a) Schematic of an ultrasound DSA reservoir, with a picture of conductive silver-coated glass microfibers dispersed in photopolymer resin. (b) Picture of microfibers that align at the nodes of a standing ultrasound wave field established between two ultrasound transducers driven by a function generator and RF amplifier. (c) Selective UV exposure initiates photopolymer resin thermosetting and fixates the aligned microfibers in place. (d) Picture of a typical composite material specimen with lines of aligned silver-coated glass microfibers (silver) in photopolymer resin (red) resulting from fabrication process steps (a)–(c). (For interpretation of the references to color in this figure legend, the reader is referred to the Web version of this article.)

Industries Inc. Conduct-O-Fil AG CLAD 12), within a photopolymer matrix (viscosity 250 cP, Makerjuice Standard). Fig. 1 (a) shows an acrylic 30.4 x 30.0  $\times$  6.0 mm reservoir with a mixture of photopolymer resin and electrically conductive microfibers, and a pair of parallel ultrasound transducers (PZT type SM111, center frequency  $f_c = 1.5$  MHz) affixed to opposing walls and separated by distance  $d = 36\lambda$ . Here,  $\lambda =$ c/f is the wavelength of the bulk ultrasound wave in the photopolymer resin, c = 1305 m/s is the sound propagating velocity in the photopolymer resin, and  $f \approx f_c$  is the operating frequency. We use a sonicator (Hielscher UP200Ht, 35.0 W, 5 min) to disperse the microfibers in the liquid photopolymer resin. Fig. 1 (b) illustrates how the microfibers align at the nodes of the standing ultrasound wave field, spaced a half wavelength apart [46,47], after we energize the ultrasound transducers with a function generator (Tektronix AFG 3102) and a radio frequency (RF) amplifier (E&I 2100L). Fig. 1 (c) depicts the SLA process, i.e., selective curing of the photopolymer resin with a UV light source (data projector ViewSonic PJD7822HDL), which fixates the aligned microfibers in place. Finally, Fig. 1 (d) shows a typical 15.00 x  $10.00 \times 0.75$ mm material specimen with lines of aligned silver-coated glass microfibers resulting from the fabrication process illustrated in Fig. 1 (a)–(c).

We fabricate composite material specimens with a weight fraction  $1.0 \le w_f \le 4.0\%$  of silver-coated microfibers, and with varying level of

alignment, to measure the effect of both parameters on the formation of a percolated microfiber network and, thus, the electrical conductivity of the material specimen. This work builds on earlier work by our research group, in which we measured and characterized macro- and microscale alignment of non-conductive carbon microfibers in photopolymer resin [48]. Leveraging the microfiber alignment characterization method of [48], we quantify the microfiber alignment using the alignment probability  $p_{\alpha}$ . This metric describes the likelihood that a cluster of microfibers aligns parallel to the ultrasound transducers and depends on the microfiber weight fraction, ultrasound transducer power, and distance between the transducers [48]. However, the fabrication process does not allow direct control of the alignment probability  $p_{\alpha}$ . Instead, we control the dimensionless ultrasound transducer input power  $P = |V|^2 t^2 / (\mu \lambda^3 \text{Re})$ (*Z*)), which determines the alignment probability  $p_a$ , and depends on the ultrasound DSA process parameters, with V the ultrasound transducer voltage, t the ultrasound exposure time,  $\mu$  the dynamic viscosity of the photopolymer resin, and Z the ultrasound transducer impedance [48].

We perform a full-factorial experiment based on two independent fabrication process parameters, the dimensionless ultrasound transducer input power P, and the microfiber weight fraction  $w_f$ , considering three (for P) and four (for  $w_f$ ) treatment levels (see Table 2). We identify treatment limits of each independent parameter such that they represent

#### Table 2

Treatment levels for independent SLA and ultrasound DSA fabrication process parameters.

Independent fabrication process	Treatment level				
parameter	1	2	3	4	
Ultrasound transducer input power <i>P</i> [-]	2.87 • 10 <sup>13</sup>	5.11 · 10 <sup>13</sup>	$1.07 \cdot 10^{14}$	N/ A	
Microfiber weight fraction w <sub>f</sub> [%]	1.0	2.0	3.0	4.0	

extreme values of the fabrication process. The microfiber weight fraction limits derive from practical considerations;  $w_f < 1.0\%$  does not reliably create a percolated microfiber network, whereas  $w_f > 4.0\%$ drastically increases the viscosity of the photopolymer and microfiber mixture and creates mechanical interlocking of the microfibers, which inhibits alignment. We select the treatment limits of *P* to fabricate material specimens with  $0.22 < p_a < 0.80$ , which we have empirically identified as the limits of this fabrication process during preliminary experiments with silver-coated glass microfibers, and in our earlier work with carbon microfibers [48].

Based on initial experiments and calculation, we require a minimum of six material specimen replications of each treatment level combination, when considering 80% statistical power and a 95% confidence interval. However, to further ensure the statistical significance of the results, we fabricate 10–20 material specimens of each treatment level combination, which results in a total of 138 material specimens.

# 2.2. Image acquisition, processing, and microfiber alignment quantification

We sand and polish the top surface of each material specimen with silicon carbide sanding paper (increasingly fine up to 1200 grit) to remove the top layer of photopolymer resin, expose the electrically conductive microfibers, and enable measuring electrical resistance along the line of aligned microfibers. Additionally, the surface preparation ensures a consistent surface finish for optical imaging. We use an optical microscope (Keyence VHX-5000) to image each material specimen with 100x magnification to quantify the microfiber alignment. Imperfections in the fabrication process or non-uniform microfiber dispersion may cause incomplete microfiber alignment. Hence, we image each material specimen covering a  $2.47 \times 2.47$  mm area (based on a convergence study), after we qualitatively observe the best microfiber alignment in each material specimen.

We quantify the alignment probability  $p_{\alpha}$  according to the method documented in Ref. [48], which we briefly summarize as follows. First, we enhance the contrast between the photopolymer resin and microfibers and convert each optical image to a binary image. Then, we employ a two dimensional fast Fourier transform (FFT) to quantify the

anisotropy in each binary image [49], such that the FFT anisotropy  $\Phi$  represents the distribution of individual microfiber alignment angles  $\theta$  in the image. Normalizing  $\Phi$  such that its integral from  $-\pi/2 \le \theta \le \pi/2$  has unit magnitude results in the probability density function of  $\theta$ , where  $\Phi = f(\theta)$ . Finally, we compute the microfiber alignment probability  $p_{\alpha}$  as

$$_{a}=\int_{Aa}^{\Delta\theta}\Phi(\theta)d\theta \tag{1}$$

Here, the alignment probability  $p_{\alpha}$  represents the likelihood that a cluster of microfibers aligns within  $\pm \Delta \theta$  of the desired alignment angle  $\theta_s$  (note that in this paper  $\theta_s$  is always such that the microfibers align parallel with the ultrasound transducers). We select  $\Delta \theta = 10^{\circ}$  because when considering the results of all the material specimens in this work, it results in a normally distributed dataset of  $p_{\alpha}$ , which is required for parametric multiple regression analysis. Fig. 2 shows a typical microfiber alignment probability measurement, where we convert (a) an optical microscopy image of a material specimen (100x magnification) into (b) a binary image, and (c) calculate  $p_{\alpha}$  according to Eq. (1).

#### 2.3. Measuring electrical resistance and calculating electrical conductivity

We paint conductive silver electrodes (SPI Supplies 05001-AB) directly onto the microfibers, exposed by sanding and polishing, along the edges of each material specimen. Fig. 3 schematically shows a typical electrical resistance measurement between opposing electrodes in the microfiber alignment direction, using a digital multimeter (Mastech MY-65), which corresponds to the "wire resistance" of an electrical conductor. Each electrode covers approximately  $2.5 \times 15 \text{ mm}^2$  and opposing electrodes are spaced L = 5 mm apart. The electrodes contact approximately 35 conductive lines of aligned microfibers, which prevents quantifying how many individual lines form a complete percolated network between the opposing electrodes. Instead, we consider each specimen as an entire percolated microfiber network. The silver coating of the microfibers is the electrically conductive component of the material specimens and, thus, we use the total volume of silver in each material specimen, derived from the microfiber weight fraction  $w_{f_1}$  to calculate electrical conductivity. We perform multiple regression analysis between the continuous electrical conductivity  $\kappa$  of the material specimens and the respective treatment levels of the microfiber weight fraction  $w_f$  and the measured alignment probability  $p_{\alpha}$ , which is a function of the non-dimensional power P. We confirm that our dataset satisfies all parametric regression analysis assumptions [50] and evaluate the best-fit model according to the root-mean-square error and *p* values (considering  $p \le 0.05$  to be statistically significant) of logarithmic, exponential, square root, inverse, and polynomial fits.

The electrical conductivity of conductive and semi-conductive materials typically ranges between  $4.35 \cdot 10^{-4} < \kappa < 6.29 \cdot 10^7$  S/m [51]. Thus, we categorize the material specimens as either electrically



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**Fig. 2.** (a) Grayscale optical microscopy image (100x magnification) of a typical material specimen. (b) Binary conversion of (a). (c) FFT anisotropy of (b), where the hatched area corresponds to the probability that a cluster of microfibers aligns within  $\pm \Delta \theta$  of the desired alignment angle  $\theta_s$ .



**Fig. 3.** Typical electrical resistance measurement, using a digital multimeter, between silver-painted electrodes in direct contact with aligned, electrically conductive silver-coated microfibers.

conductive or insulating depending on whether the electrical conductivity is larger or smaller than  $4.35 \cdot 10^{-4}$  S/m. We perform logistic regression analysis between the categorical classification of an electrical conductor or insulator of all material specimens and the respective treatment levels of  $w_f$  and  $p_{\alpha}$ , thus relating whether a material specimen is electrically conductive or insulating to the fabrication process parameters. Hence, the best-fit logistic regression model predicts whether a material specimen is electrically conductive, according to the model  $X^2$ , McFadden  $R^2$ , and p values. We confirm that the model complies with logistic regression assumptions [52] and evaluate logarithmic, exponential, square root, inverse, and polynomial fits.

#### 3. Results and discussion

#### 3.1. Electrically conductive versus insulating

Fig. 4 shows an overview of all material specimens in the fullfactorial experiment. The rows and columns indicate different treatment levels of the microfiber weight fraction  $w_f$  and dimensionless power *P*, respectively (see Table 2). We list the number of electrically conductive material specimens, classified as electrical conductors or insulators, compared to the total number of specimens of each treatment level combination. We color-code each combination as a function of the fraction of electrically conductive material specimens and include an image of a typical material specimen with lines of aligned conductive microfibers fabricated using each treatment level combination.

A percolated network of electrically conductive microfibers must exist within the insulating polymer matrix material for the material specimen to conduct electricity. Percolation depends on the density of microfibers that agglomerate at the nodes of the standing ultrasound wave field during the ultrasound DSA process, which in turn depends on both the microfiber weight fraction  $w_f$  and the alignment probability  $p_\alpha$ (controlled by the non-dimensional power *P*). Fig. 4 shows that the fraction of electrically conductive material specimens increases with increasing microfiber weight fraction  $w_f$  and non-dimensional power *P*. While we did not determine limits of the fabrication process parameters that guarantee electrical conductivity, almost all specimens with *P* >  $5.11 \cdot 10^{13}$  and  $w_f > 3.0$  show a complete percolated network of



**Fig. 4.** Overview of all material specimens in the full-factorial experiment, showing the fraction of electrically conductive specimens for each process parameter treatment level combination, including an image of a typcial specimen.

conductive microfibers. We also observe that the lines of microfibers show increased alignment with increasing P and increased density with both increasing  $w_f$  and P. Physically, increasing P increases the alignment of the microfibers because it increases the amplitude of the ultrasound standing wave and, thus, the corresponding acoustic radiation force that drives the microfibers to the nodes of the standing ultrasound wave field. Additionally, increasing the  $w_f$  increases the number of microfibers mixed in the matrix material and, thus, the likelihood that individual microfibers contact each other to form a long-range conductive pathway through the material specimen, independent of their alignment.

Fig. 5 shows optical microscopy images of material specimens fabricated with constant *P* and different  $w_f$  to illustrate the importance of the interaction between *P* and  $w_f$ . We observe from Fig. 5 (a) that even with high *P*, and therefore well-aligned microfibers, gaps might exist locally between adjacent conductive microfibers when the microfiber weight fraction is low ( $w_f = 1.0\%$ ), preventing a percolated network of microfibers and, thus, electrical conductivity. Additionally, we observe from Fig. 5 (b) that no gaps exist between microfibers when the microfiber weight fraction is high ( $w_f = 4.0\%$ ), even if the alignment of the individual microfibers is imperfect. Note also the substantially thicker lines of aligned microfibers with  $w_f = 4.0\%$  compared to  $w_f = 1.0\%$ , thus locally increasing the microfiber density.

Equation (2) shows the best-fit logistic regression model of the categorical classification of an electrical conductor or insulator of all the



**Fig. 5.** (a) Electrically insulating material specimen because gaps exist locally between adjacent microfibers due to the low microfiber weight fraction ( $w_f$  = 1.0%), despite showing well-aligned electrically conductive microfibers. (b) Electrically conductive material specimen ( $\kappa$  = 153 S/m) because no gaps exist between adjacent microfibers due to high microfiber weight fraction ( $w_f$  = 4.0%) and well-aligned electrically conductive microfibers.

material specimens as a function of the microfiber weight fraction  $w_f$  and the measured alignment probability  $p_{\alpha}$ , with  $X^2 = 88.3$ , McFadden  $R^2 =$ 0.50, and p values of  $2.76 \cdot 10^{-9}$  and  $6.08 \cdot 10^{-7}$  for  $w_f$  and  $p_{\alpha}$ , respectively. In Eq. (2),  $p_{conductive} = 1$  when the material specimen is electrically conductive, and  $p_{conductive} = 0$  when it is electrically insulating. We note that a McFadden  $R^2$  of 0.2–0.4 is approximately equivalent to an  $R^2$  of 0.7–0.9 for a linear function [53], indicating that the logistic regression model shows an excellent fit of the experimental data.

$$p_{conductive} = \frac{e^{-17.24 + 2.14w_f + 7.60p_a}}{1 + e^{-17.24 + 2.14w_f + 7.60p_a}}$$
(2)

Fig. 6 shows the probability that a material specimen fabricated with the combined SLA and ultrasound DSA process is electrically conductive  $p_{conductive}$ , as a function of the alignment probability  $p_{\alpha}$ , for different values of the microfiber weight fraction  $w_f$  (identified with different color lines and marker types). The solid lines represent Eq. (2) for different values of  $w_f$ , whereas the markers indicate the individual experimental data points, discretely categorized as electrically conductive ( $p_{conductive} = 1$ ) or insulating ( $p_{conductive} = 0$ ) and, thus, not considering continuous values of the electrical conductivity.

Fig. 6 shows that the probability that a material specimen with lines

of aligned conductive microfibers is electrically conductive, increases with increasing microfiber alignment probability  $p_{\alpha}$  and weight fraction  $w_f$ , respectively. The experimental data matches this trend, illustrated by the different markers at  $p_{conductive} = 1$  and  $p_{conductive} = 0$ , respectively. From Fig. 6 we also observe that specimens with  $w_f = 1.0\%$  or  $w_f = 4.0\%$ show higher deviation between theoretical and experimental  $p_{conductive}$ values than specimens with  $w_f = 2.0\%$  and  $w_f = 3.0\%$  because they are heavily skewed towards  $p_{conductive} = 0$  and  $p_{conductive} = 1$ , respectively.

We further illustrate the results of Fig. 6 by showing physical data from the material specimens in Fig. 7 (increasing the microfiber weight fraction  $w_f$ ) and Fig. 8 (increasing the microfiber alignment probability  $p_\alpha$ ). Figs. 7 and 8 (a)–(c) show schematic representations of the electrically conductive microfibers in the matrix material with increasing alignment probability  $p_\alpha$  and microfiber weight fraction  $w_f$ , respectively, whereas Figs. 7 and 8 (d)–(i) show optical images with different magnification that illustrate the effects of  $p_\alpha$  and  $w_f$  on the formation of a percolated microfiber network.

Fig. 7 (a)–(c) illustrate that increasing  $w_f$  creates increasingly closely packed individual microfibers (black), which are more likely to make contact to form a percolated network of electrically conductive microfibers (red). Fig. 7 (d)–(f) show that the density of a single line of aligned microfibers increases with increasing  $w_{\rm f}$  again increasing the likelihood that electrically conductive microfibers make contact and form a percolated network. Similarly, Fig. 7 (g)-(i) show multiple lines of aligned microfibers. We observe that the thickness of these lines of aligned microfibers increases with increasing  $w_f$  because more microfibers agglomerate at the nodes of the standing ultrasound wave. This again increases contact between microfibers and the likelihood of forming a percolated network. Fig. 8 (a)–(c) illustrate that increasing the alignment probability  $p_{\alpha}$  increases the likelihood that individual microfibers (black) make contact (red) and form a percolated network. Fig. 8 (d)–(f) show that the density of a single line of aligned microfibers increases with increasing  $p_{\alpha}$ , again increasing the likelihood that electrically conductive microfibers make contact and form a percolated network. Similarly, Fig. 8 (g)-(i) show multiple lines of aligned microfibers. We observe that the density of these lines of aligned microfibers increases with increasing  $p_{\alpha}$  because increased alignment of the microfibers exists at the nodes of the standing ultrasound wave. This again increases contact between microfibers and the likelihood of forming a percolated network.

## 3.2. Continuous electrical conductivity

Fig. 9 shows the electrical conductivity  $\kappa$  of the electrically conductive material specimens from the full-factorial experiment as a function of the measured microfiber alignment probability  $p_{\alpha}$ . Marker types and colors indicate different microfiber weight fractions  $w_{f}$ .

From Fig. 9 we observe that  $p_{\alpha}$  increases and then decreases with increasing  $w_f$ , for  $w_f \ge 1.0$  and  $w_f \ge 2.0$ , respectively. This suggests that the nodes of the ultrasound wave field saturate with microfibers when  $1.0 < w_f < 2.0$ , causing microfibers to entangle and preventing additional microfibers from aligning at the nodes. The electrical conductivity  $\kappa$  of the conductive material specimens varies from 31 to 793 S/m, but statistical analysis does not reveal significant trends within the dataset of electrically conductive material specimens as a function of fabrication process parameters. This means that although  $p_{\alpha}$  and  $w_f$  are critical in predicting whether a material specimen will be electrically conductive (see Eq. (2)), these process parameters do not significantly affect the magnitude of the electrical conductivity of a material specimen within an existing percolated network of electrically conductive fibers. Once an electrically conductive pathway exists, electrical current can flow independent of the shape (alignment) or geometry (density) of that pathway.

Although no publications in the open literature characterize the electrical conductivity of polymer matrix composite materials with aligned microfibers as a function of the microfiber weight fraction  $w_f$ 

- 200 μm

400 µm

Fully

percolated

network



Fig. 6. Probability that a material specimen is electrically conductive  $p_{conductive}$  as a function of microfiber alignment probability  $p_a$  and weight fraction  $w_{f_1}$  also showing each individual experimental datapoint.



Fig. 7. (a)-(c) Schematic illustrating that a percolated network of discontinuous conductive microfibers forms with increasing microfiber weight fraction  $w_{f}$ . (d)–(f) Optical images of individual microfibers, from a line of aligned microfibers, illustrating that increasing  $w_f$  causes microfibers to make contact and form a percolated network. (g)-(i) Optical images of sections of material specimens with multiple lines of aligned microfibers, illustrating that increasing  $w_f$  causes a higher microfiber density at the nodes of the standing ultrasound wave, which promotes the formation of a percolated network of electrically conductive microfibers.

conductive microfibers forms with increasing alignment probability  $p_{q}$ . (d)–(f) Optical images of individual microfibers, from a line of aligned microfibers, illustrating that increasing  $p_{\alpha}$  causes microfibers to make contact and form a percolated network. (g)-(i) Optical images of sections of material specimens with multiple lines of aligned microfibers and constant  $w_{\mathrm{f}}$ , showing that increasing  $p_{\alpha}$  increases the microfiber density at the nodes of the standing ultrasound wave, which promotes the formation of a percolated network of electrically conductive microfibers.



**Fig. 9.** Electrical conductivity  $\kappa$  as a function of microfiber alignment probability  $p_{a}$ , for different values of the microfiber weight fraction  $w_{f}$ .

and alignment probability  $p_{\alpha}$ , several groups have published related studies. Our findings agree with the results documented by Melchert et al., who fabricated flexible polymer matrix composite materials with silver-coated glass and uncoated carbon microfibers aligned using ultrasound DSA [42]. They reported a maximum electrical conductivity of  $\kappa = 5000$  and 10 S/m, for silver-coated glass and uncoated carbon microfibers, respectively, and found that the magnitude of  $\kappa$  remained almost constant, independent of wf. Oliva-Avilés et al. fabricated polymer matrix composite materials with aligned MWCNTs using an electric field, and reported that the electrical conductivity  $\kappa$  increased with increasing microfiber weight fraction for  $0.1 \le w_f \le 0.5\%$  with a maximum conductivity  $\kappa$  of approximately 0.05 S/m (for  $w_f = 0.5\%$ ) [25], which is four orders of magnitude lower than the material specimens we have fabricated for this paper. We speculate that this difference is because the silver-coated microfibers are more electrically conductive than the uncoated MWCNTs. Similarly, Ma et al. aligned nickel-infused CNTs in an epoxy matrix using a magnetic field, and measured that the electrical conductivity  $\kappa$  increased with increasing weight fraction for  $0.5 < w_f < 5.0\%$  with maximum  $\kappa$  of  $4 \cdot 10^{-3}$  S/m [36], which is inconsistent with our findings. Postiglione et al. printed electrically conductive PLA composite materials with aligned MWCNTs and also measured that electrical the conductivity  $\kappa$  increased with increasing MWCNT weight fraction, for  $0.5 < w_f < 10.0\%$ , up to approximately 50 S/m [37], which is on the same order of magnitude as composite materials we fabricated for this paper. Finally, Ladani et al. fabricated epoxy composite materials with carbon nanofibers (CNFs) or graphene nanoplatelets (GNPs) aligned using an electric field and also measured that the electrical conductivity  $\kappa$  increased with increasing filler weight fraction  $w_{f_2}$  up to approximately 0.01 S/m and  $10^{-6}$  S/m, for CNFs and GNPs, respectively [5]. Furthermore, it is evident that electrical conductivity depends on the filler material properties, which explains differences between our work and that of other groups.

Characterizing the probability that a composite material is electrically conductive as a function of the fabrication process parameters, including the microfiber weight fraction  $w_f$  and alignment probability  $p_{a}$ , is an important step towards using ultrasound DSA as a fabrication process for engineered polymer matrix composite materials with designer electrical properties. For instance, by leveraging the regression model in this paper, we can estimate the minimum microfiber weight fraction  $w_f$  and microfiber alignment probability  $p_{\alpha}$  required to fabricate an electrically conductive material specimen. Such materials are of interest to a myriad of engineering applications, including flexible electronics, chemical or biological sensors, and stretchable strain sensors, amongst others. Furthermore, this paper shows that the combined SLA and ultrasound DSA method enables the fabrication of macroscale material specimens, thus demonstrating the dimensional scalability of the technique. Limitations of the dimensional scalability include input power to the ultrasound transducers, as this might locally heat the photopolymer resin and cause boiling, and photopolymer viscosity, which affects ultrasound wave attenuation and the magnitude of viscous drag forces acting on the filler material. Additionally, increasing the weight fraction of the filler material increases the viscosity of the photopolymer/filler material mixture and may change the curing characteristics of the photopolymer.

We also emphasize that ultrasound DSA functions independent of the material properties of the filler material and, thus, while we use silvercoated microfibers for this study, one could use the fabrication process with any other type of filler material and repeat the study to evaluate electrical conductivity. While the results might change, the method and approach documented in this paper remain valid, independent of the specific material combination.

#### 4. Conclusions

A percolated network of electrically conductive microfibers is required to obtain long-range electrical conductivity throughout an engineered polymer matrix composite material. Percolation is driven by the density of microfibers along the conductive path. Ultrasound DSA aligns microfibers at the nodes of a standing ultrasound wave and the microfiber weight fraction determines the number of microfibers that agglomerates at the nodes of the standing ultrasound wave. Thus, the density of microfibers along the conductive path depends on both microfiber alignment and microfiber weight fraction. Specifically:

- 1. The percolation threshold decreases with increasing microfiber alignment probability because microfiber density at the nodes of the standing ultrasound wave increases with increasing alignment probability, which increases contact between neighboring microfibers.
- 2. The alignment probability required for electrical conductivity decreases with increasing microfiber weight fraction because adding more microfibers to a composite material specimen increases microfiber density and, therefore, increases contact between neighboring microfibers, independent of alignment probability.

These results agree with results documented by others using different fabrication methods, as highlighted in the introduction and discussion of this paper. However, we emphasize that the combined ultrasound DSA and SLA fabrication process offers flexibility in terms of specimen geometry through the SLA process, spatial arrangement and alignment of the discontinuous filler material through the ultrasound DSA process, and dimensional scalability through the combination of both.

We also conclude that although microfiber weight fraction and alignment probability are crucial in predicting if a composite material specimen will be electrically conductive, the fabrication process parameters do not significantly affect the magnitude of electrical conductivity of a material specimen with an existing percolated network. Understanding the relationship between the ultrasound DSA process parameters and the resulting electrical conductivity of a composite material specimen is an important step towards fabricating macroscale engineered polymer matrix composite materials with embedded percolated networks of aligned and electrically conductive microfibers for use in a myriad of engineering applications.

#### Author statement

KN and BR designed the experiments, KN performed the experiments, KN and BR analyzed the data and wrote the manuscript.

## Declaration of competing interest

The authors declare that they have no known competing financial interests or personal relationships that could have appeared to influence the work reported in this paper.

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